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BACKGROUND

- Electromagnetic and electrical stimulation can modulate neural activity in the sensorimotor system.
- Stimulation of the brain and spinal cord causes muscles to produce motor-evoked potentials (MEPs).
- The recruitment curve illustrates the relationship between stimulation intensity and MEP size.

Problem: Sparse data due to experimental constraints poses a challenge for accurately estimating curves and their key parameters including threshold, S_{50} , slope, and saturation.

Approach: A new hierarchical Bayesian framework is introduced.

METHODS

RECRUITMENT CURVE ESTIMATION

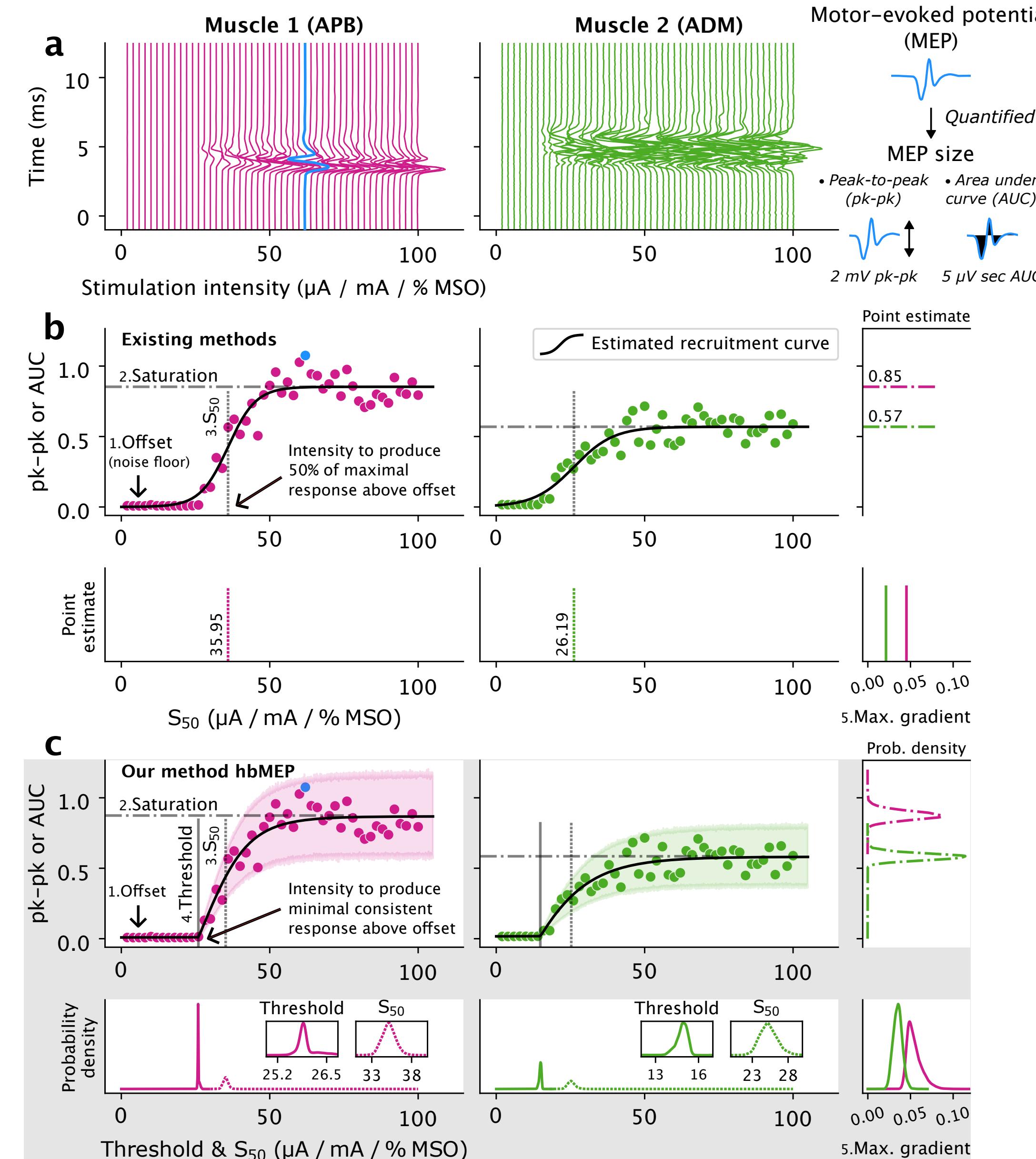


Fig. 1. Hierarchical Bayesian estimation of recruitment curves. (a) Motor-evoked potentials (MEPs). (b) Recruitment curves estimated using sigmoid function lack threshold estimate. (c) Estimated using new rectified-logistic function within a hierarchical framework. Shading represents 95% highest density intervals (HDI).

SYNTHETIC DATA GENERATION

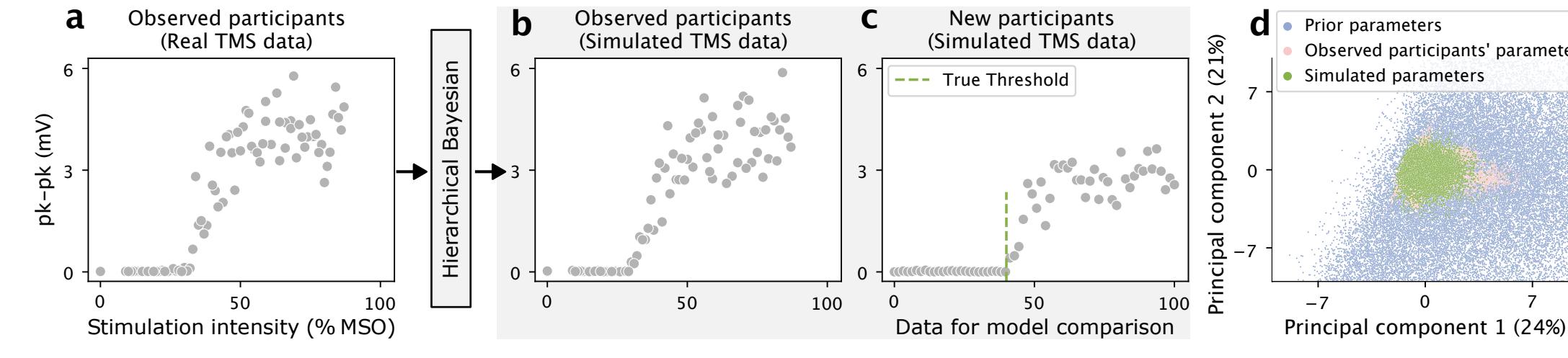


Fig. 2. Hierarchical model simulates high-fidelity synthetic TMS data. (a) Example participant from human TMS data. (b) Hierarchical model can replicate observed participant. (c) Example synthetic participant simulated conditioned on estimated population-level parameters for model comparison. (d) Principal component analysis plot shows large overlap between simulated data parameters (green) and parameters estimated from observed data (pink).

ACKNOWLEDGEMENTS

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YIELDS ACCURATE AND ROBUST ESTIMATES

IMPROVED ACCURACY

Fig. 3. (a-b) Standard hierarchical Bayesian model improves threshold estimation accuracy over non-Bayesian and non-hierarchical models on simulated data. **(c-d)** Bayesian estimation is more powerful when detecting a shift in the threshold compared to frequentist testing.

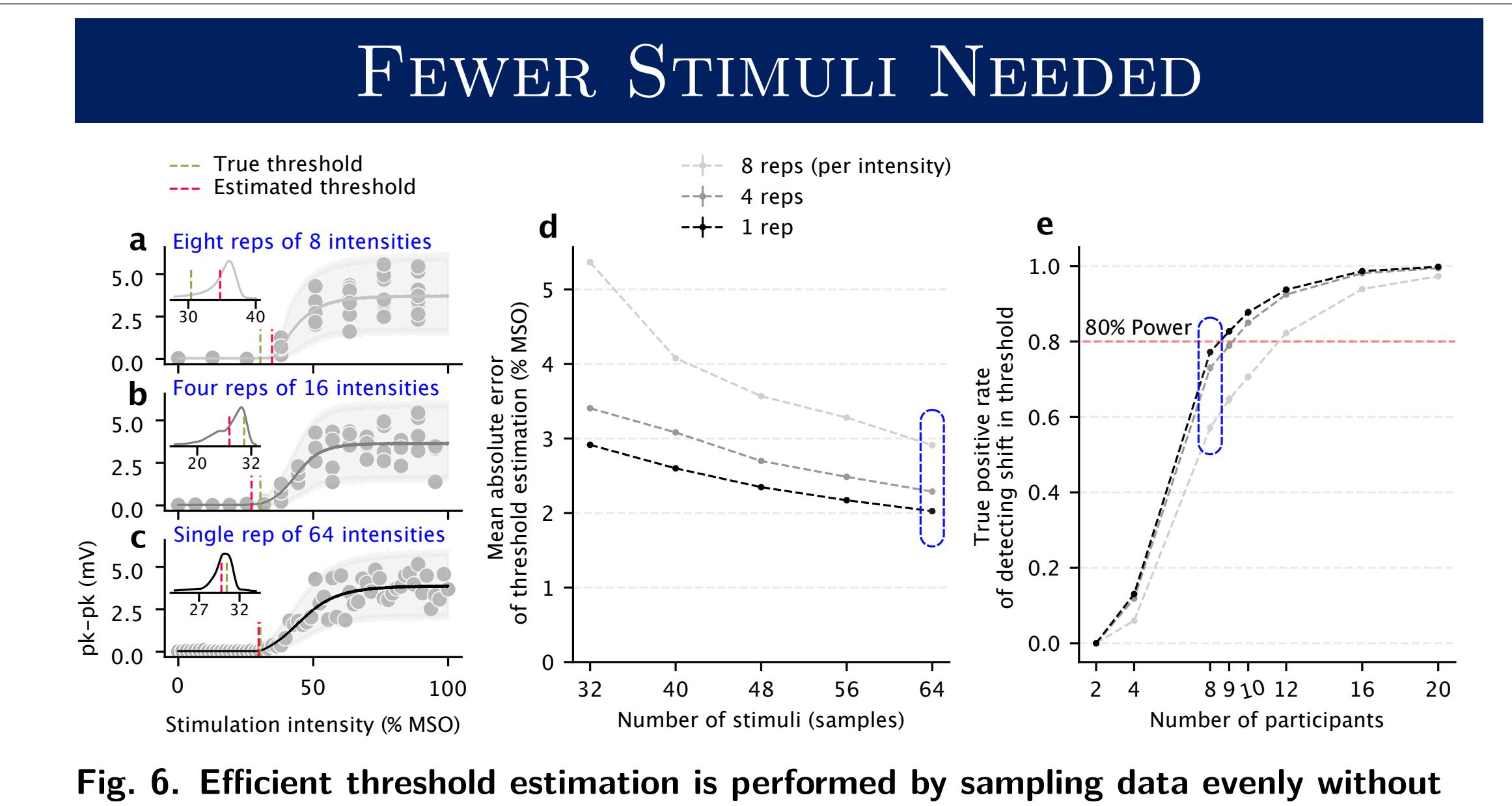
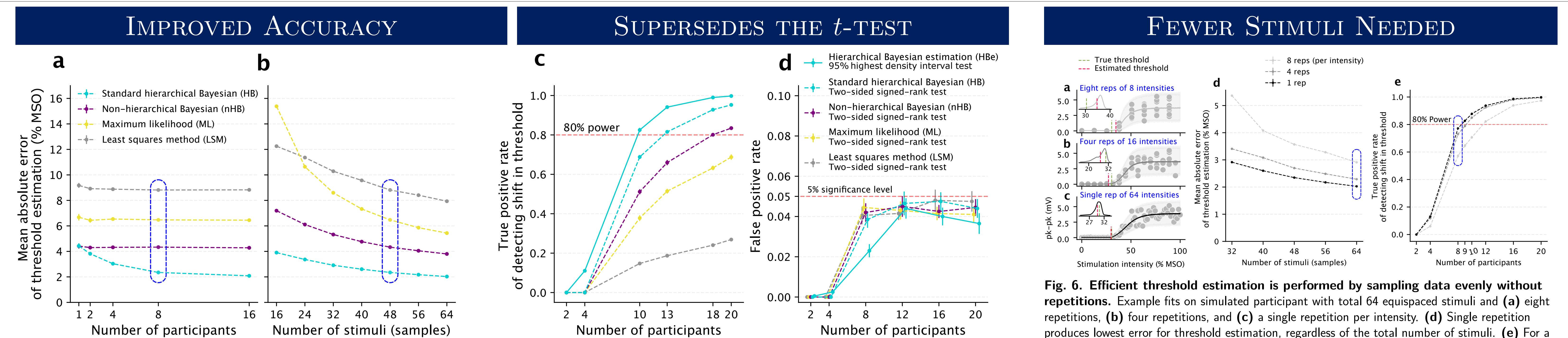


Fig. 6. Efficient threshold estimation is performed by sampling data evenly without repetitions. Example fits on simulated participant with total 64 equispaced stimuli and (a) eight repetitions, (b) four repetitions, and (c) a single repetition per intensity. (d) Single repetition produces lowest error for threshold estimation, regardless of the total number of stimuli. (e) For a fixed total of 64 stimuli, fewer repetitions require fewer participants to achieve 80% power when detecting shift in threshold from pre- to post-intervention phase.

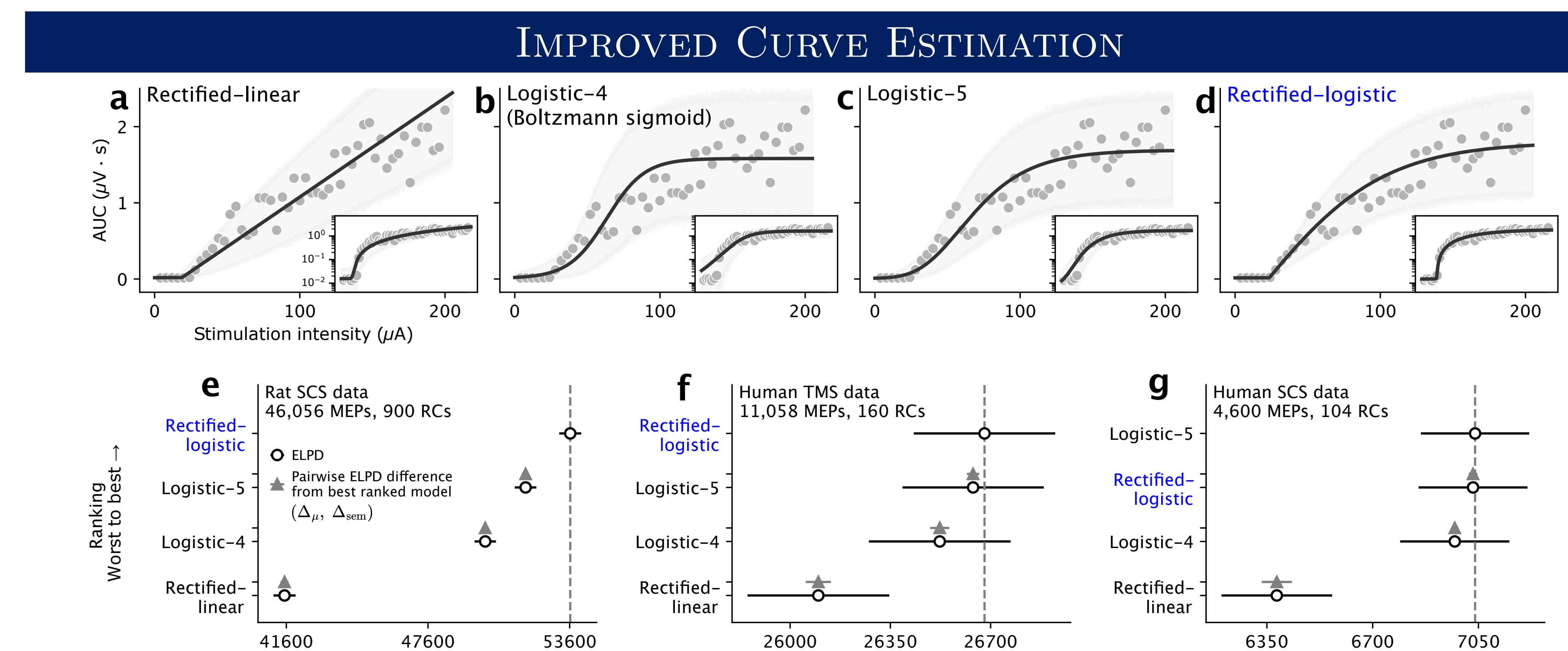


Fig. 4. Cross-validation on real Spinal Cord Stimulation (SCS) and Transcranial Magnetic Stimulation (TMS) data. Rectified-logistic function outperforms conventional logistic alternatives in predictive performance based on leave-one-out cross-validation [1], while having the unique advantage of estimating threshold, curvature and saturation.

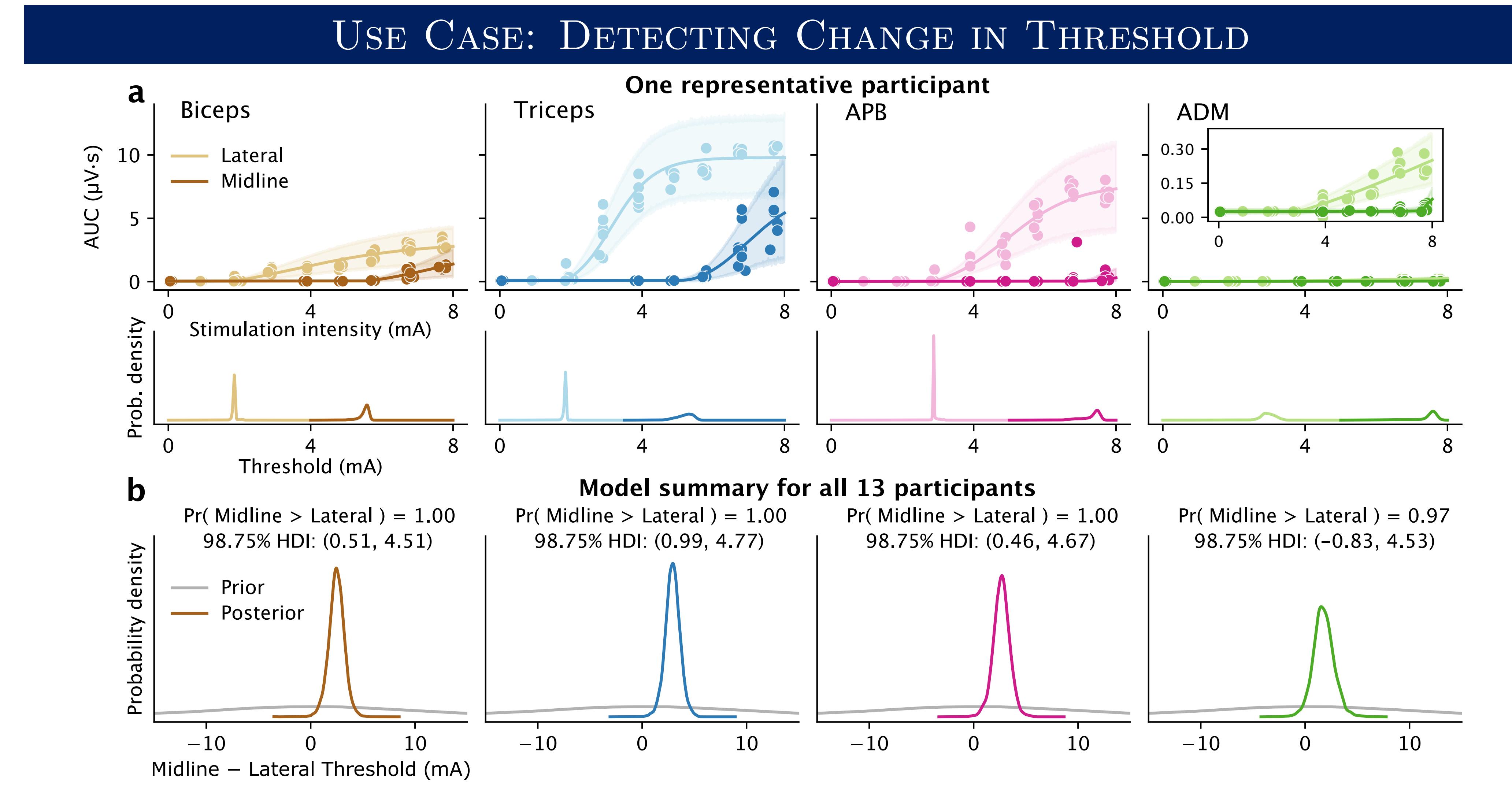


Fig. 5. Comparison of midline versus lateral stimulation thresholds on human epidural SCS data. (a) Example participant with lateral (light) and midline (dark) stimulation. Inset: zoom to show presence of threshold, despite small MEP size. (b) Difference between midline and lateral thresholds summarized by model across $N = 13$ participants suggests strong evidence in favor of lateral stimulation resulting in lower thresholds and being more effective, a known effect [2].

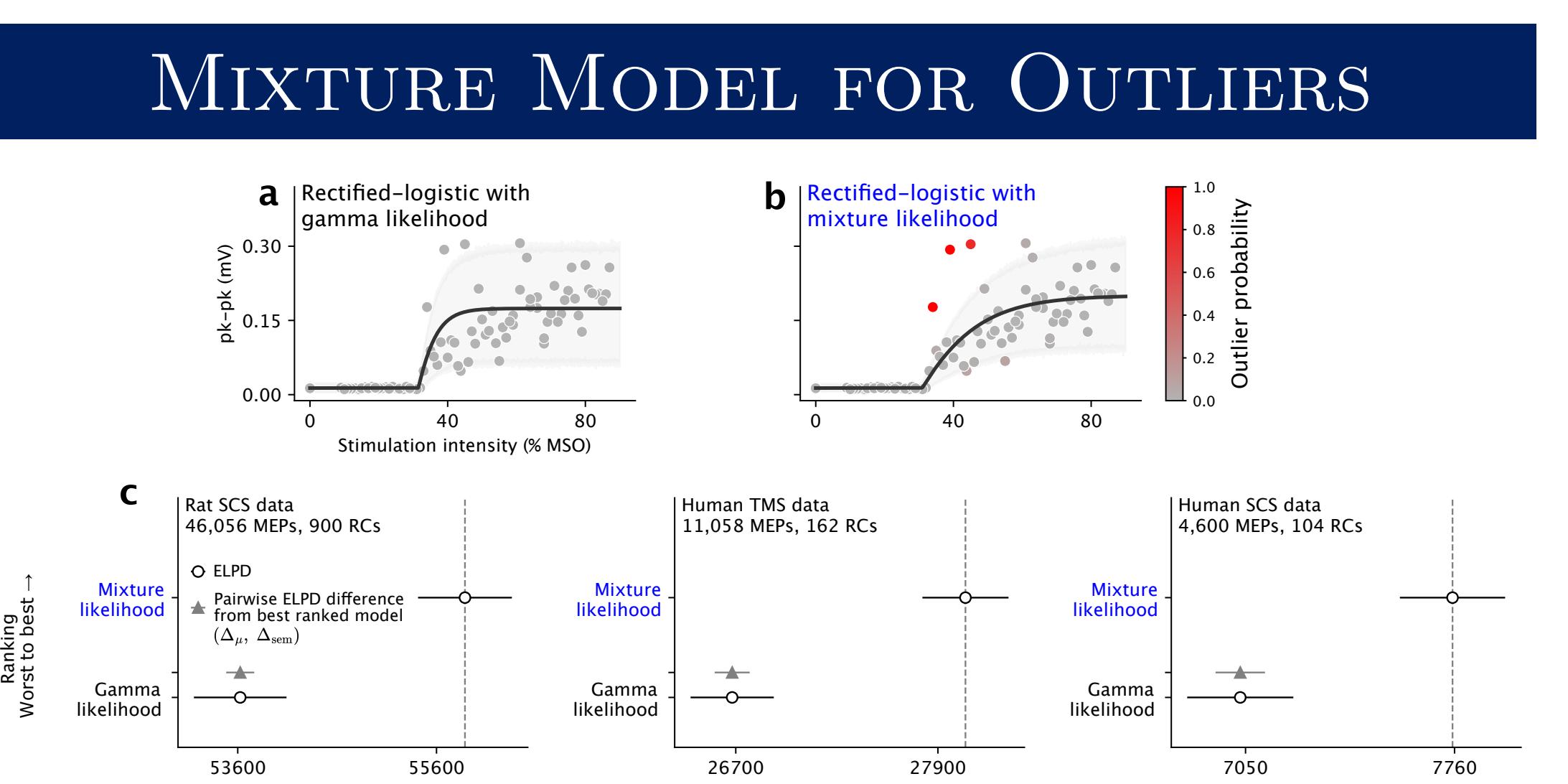


Fig. 7. Mixture model accounts for outliers and further improves predictive performance on all datasets. (a) Example overestimated growth rate due to the presence of outliers. (b) Mixture extension of the likelihood model is more robust to outliers. (c) Leave-one-out cross-validation.

CONCLUSION

- Threshold estimation:** Rectified-logistic function allows estimation of motor threshold, which is independent of observed saturation, as opposed to S_{50} estimated with logistic functions.
- Improved accuracy and power:** Partial pooling within a hierarchical framework provides more reliable and accurate estimates, which also translates into increased statistical power when detecting changes in threshold.
- Reduced experimental burden:** The framework lowers experimental burden by reducing the number of stimuli required per participant while maintaining accuracy and simultaneously increasing the number of muscles across which these insights are obtained.
- Validation across different stimulation modalities:** The framework is validated across spinal cord stimulation (SCS) and transcranial magnetic stimulation (TMS), highlighting its utility in different experimental contexts.
- Future work:** This method can extend into an adaptive algorithm for efficient collection of data across multiple muscles during live SCS and TMS experiments.

REFERENCES

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